

Nanotechnology and nuclear medicine; research and preclinical applications

Abstract

The birth of nanotechnology in human society was around 2000 years ago and soon found applications in various fields. In this article, we highlight the current status of research and preclinical applications and also future prospects of nanotechnology in medicine and in nuclear medicine. The most important field is cancer. A regular nanotechnology training program for nuclear medicine physicians may be welcome.

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Introduction

Nanotechnology is the manipulation of matter on an atomic and molecular scale to prepare new structures, devices and materials. In general, nanotechnology uses materials sized between 1 and 100 nanometres [1]. The birth of nanotechnology in human society was around 2000 years ago, when sulfide nanocrystals were used as hair dye and gold nanoparticles for coloring glass by ancient Greeks and later by Romans [2, 3]. The word "nanos" in Greek means dwarf [2, 3]. Feynman first presented the modern concept of nanotechnology in 1959 [2]. Smalley, who was awarded the Nobel Prize in chemistry for the discovery of a new carbon nanotube, defined nanotechnology "as the art and science of building stuff that does stuff at the nanometer scale" [3]. The interdisciplinary nature of nanotechnology has given it a fundamental influence in various fields, especially medical science. Nanomedicine is defined as the knowledge and skill of manipulating and exploiting the unique chemical, physical, electrical, optical, and biological attributes of natural or synthesized material at the nano-sized scale for various medical purposes, such as opportune prevention, early detection, and targeted treatment of disease [4-9]. Potential nanotargeted radionuclides for diagnosis (Table 1) and treatment (Table 2) are based on the physical half-life, decay mode, the emission properties, and also their tissue penetration range.

Applications of nanotechnology in nuclear medicine can be found in areas of diagnostics, therapeutics, theranostics, and regenerative medicine, as described below (Fig. 1).

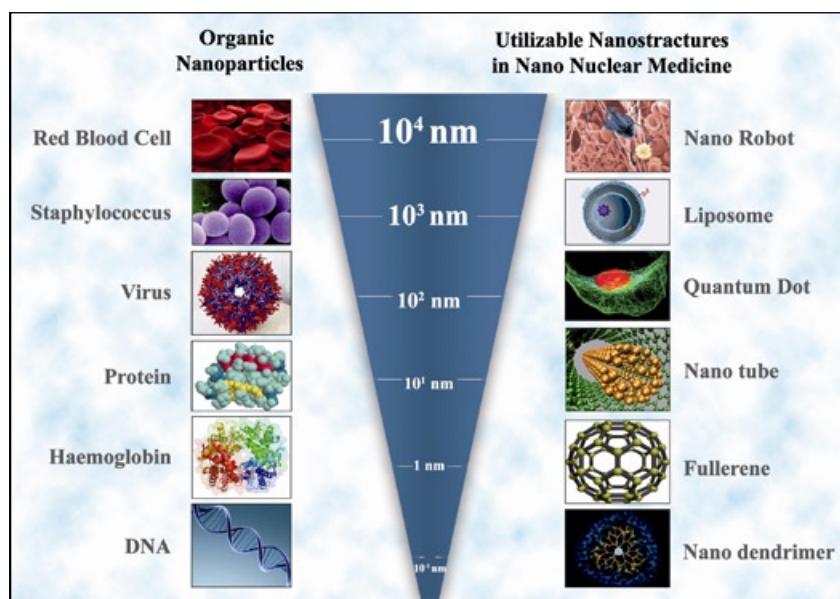


Figure 1. The organic nanoparticle as compared with utilizable nanostructures in nano-nuclear medicine

**Majid Assadi¹ MD,
Kolsoom Afrasiabi¹ MD,
Iraj Nabipour² MD,
Mohammad Seyedabadi¹ PhD**

1. The Persian Gulf Nuclear Medicine Research Center, Bushehr University of Medical Sciences, Bushehr, Iran
2. The Persian Gulf Tropical Medicine Research Center, Bushehr University of Medical Sciences, Bushehr, Iran

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- Regenerative medicine

Correspondence address:

Majid Assadi, MD
The Persian Gulf Nuclear Medicine Research Center, Bushehr University of Medical Sciences, Bushehr 3631, Iran
Tel: 0098-771-2580169
Fax: 0098-771-2541828
E-mail: assadipoya@yahoo.com, asadi@bpums.ac.ir

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Table 1. Profiles of potential radionuclides for nanotargeted imaging

Radionuclide	Emission type	E max(keV)	Half-life	Production	Imaging type
^{99m} Tc	γ	140	6.0h	⁹⁹ Mo/ ^{99m} Tc-generator	SPET
¹¹¹ In	Auger, γ	171, 245	67.2h	¹¹¹ Cd (p, n) ¹¹¹ In	>>
⁶⁷ Ga	γ	93, 184, 300, 393	78.3h	⁶⁸ Zn (n, p) ⁶⁷ Ga	>>
¹³¹ I	γ (81.2%), β	284, 364, 637	8.0 days	¹³⁰ I(n, γ) ¹³¹ Te (β) ¹³¹ I	>>
¹²³ I	Auger, γ	159	13.2h	¹²¹ Sn (α, 2n) ¹²³ I	>>
^{125m} Te	γ	-	57.4 days	¹²⁵ Sn(β-) ¹²⁵ Sb(β-)	>>
¹¹ C	Positron	960	20.4min	¹⁴ N (p,α) ¹¹ C	PET
¹⁵ O	>>	1720	2.07min	¹⁴ N (d,n) ¹⁵ O	>>
¹³ N	>>	1190	9.96min	¹⁶ O (p,α) ¹³ N	>>
¹²⁴ I	>>	Eβ+ 2134, 1533	100.2h	¹²⁴ Te(p, n) ¹²⁴ I	>>
¹⁸ F	>>	Eβ+ 635	1.83h	¹⁸ O (p, n) ¹⁸ F	>>
⁷⁶ Br	>>	Eβ+ 3941	16.0h	⁷⁶ Se(p, n) ⁷⁶ Br	>>
⁶⁴ Cu	>>	Eβ+ 656	12.7h	⁶⁴ Ni(p, n) ⁶⁴ Cu	>>

EB , E max of β; P, proton; a, alpha; n, neutron

Table 2. Profiles of potential radionuclides for nanotargeted treatment

Radionuclide	Emission type	E max (MeV)	Half-life	Production	R max (mean)
¹¹¹ In	Auger,γ	0.42	67h	¹¹¹ Cd (p, n) ¹¹¹ In	2–500nm
⁶⁷ Cu	β	0.19	2.6 d	⁶⁴ Ni(a, p) ⁶⁷ Cu	2.2mm (0.7mm)
⁹⁰ Y	β	2.28	64.1h	⁹⁰ Sr/ ⁹⁰ Y-generator	12mm (2.8mm)
¹³¹ I	γ (81.2%), β	0.28, 0.36, 0.64	8 d	¹³¹ Te (β) ¹³¹ I	2.4mm (0.8mm)
¹⁸⁸ Re	β, γ (15.1%)	2.12	17h	¹⁸⁸ W/ ¹⁸⁸ Re-generator	11mm (2.4mm)
¹⁸⁶ Re	β, γ (9.4%)	1.07	89.2h	¹⁸⁵ Re (n, γ) ¹⁸⁶ Re	5mm (1.8mm)
²²⁵ Ac	α	5.83, 5.79, 5.79, 5.73	10 d	²²⁵ Ra-generator	40–80μm
¹⁷⁷ Lu	β	0.49	161h	¹⁷⁶ Lu (n, γ) ¹⁷⁷ Lu	1.6mm (0.67mm)
¹⁶⁶ Ho	β, γ (6.7%)	1.853	26.9h	¹⁶⁵ Ho (n, γ) ¹⁶⁶ Ho	10.2mm
⁸⁹ Sr	β	1.463	52.7 d	⁸⁸ Sr (n,γ) ⁸⁹ Sr	3mm
³² P	β	1.71	14.3 d	³² S (n,p) ³² P or ³¹ P (n, γ) ³² P	8.7mm
²¹¹ At	α	5.87	7.2h	Accelerator	60–80μm
²¹³ Bi	α	5.869	45.7min	²²⁵ Ra-generator	50–80μm
²²³ Ra	α	-	11.4 d	²²⁷ Ac-generator	-
²²⁴ Ra	α	-	3.6 d	generator	-
¹⁰³ Pd	X-ray	0.021	17.0 d	accelerator	-
¹⁹⁸ Au	β	0.96	2.7 d	cyclotron	-

EB , E max of β; P, proton; a, alpha; n, neutron.

Research and preclinical applications of nanotechnology

Nanomaterials can improve diagnostic imaging techniques even at the level of single cells before overall symptoms appear [7, 10, 11]. Fusion of nanomaterials with molecular imaging devices permits diagnostic and dynamic processes at the molecular level [7]. A single nanoparticle can be tagged with various imaging agents and different targeting ligands can be constructed on similar nanoparticles to introduce selectivity. The ability of nanoparticles to bypass biological barriers enhances targeting efficacy (Fig. 2) [12]. Finally, radio-labeled nanoparticles remain stable under many physiological conditions [13].

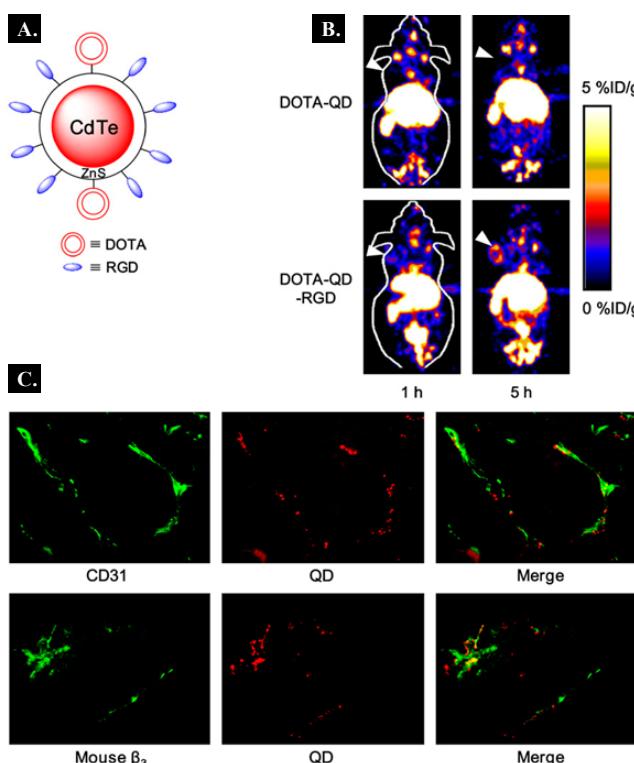


Figure 2. Dual-modality PET/NIRF imaging of integrin $\alpha v\beta 3$ in vasculature of tumor. **(A)** A schematic figure of the dual-modality PET/NIRF probe. **(B)** NIRF (after injection of QD-RGD) and coronal microPET (after injection of ^{64}Cu -DOTA-QD-RGD) views of a U87MG tumor bearing mice. **(C)** Outstanding overlay between CD31 and QD fluorescence, as well as between murine $\beta 3$ and QD fluorescence, verified that DOTA-QDRGD principally targeted integrin $\alpha v\beta 3$ on the tumor vasculature. (Adapted with permission from [12]. ©2007 Society of Nuclear Medicine)

The main advantages of radionuclide-based molecular imaging modalities and of other imaging techniques (e.g. molecular magnetic resonance imaging (mMRI)) are sensitivity, and the possibility of being quantitative, while the main disadvantage is the low resolution typically >1mm [14, 15]. Multi-modality imaging using nanoparticles could have a better intrinsic and extrinsic resolution [1, 15] and higher accuracy [12]. Furthermore, multiple imaging agents can be used in multiplexing-modal imaging, simultaneously (Fig. 3) [16]. The enormous surface area of nanoparticles has made them one of the ideal tools to make use of the advantages of multifunctional imaging. Thus nanometric structures can be considered ideal devices for multifunctional imaging programs [17].

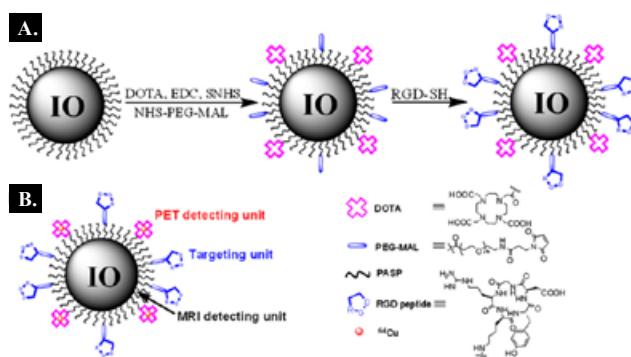


Figure 3. (A) Synthesis of PET/MRI dual functional probe DOTA-IO-RGD. DOTA-IO was produced in the same way except that no RGD peptide was used. (B) Illustration of PET/MRI probe founded on IO nanoparticle. (Adapted with permission from [16]. ©2008 Society of Nuclear Medicine)

A variety of imaging labels such as superparamagnetic iron oxide (SPIO) nanoparticles, quantum dots (QDs), and micro-bubbles have been used for nuclear imaging of tumor angiogenesis [12][18-21]. Others have suggested that molecular imaging of tumor angiogenesis could be nanomaterial based and be applied also in atherosclerosis and cancer [12].

Multi-labeling of nanoparticles improves contrast-to-noise ratio and eliminates the partial volume effect that is considered a disadvantage of traditional nuclear medicine in the detection of atherosclerosis plaques. Exposed atherosclerosis plaques are an important cause of acute cardiovascular events and sudden death in asymptomatic patients [22]. Furthermore, exchange of high density lipoprotein (HDL) cores with synthetic nanomaterials such as QDs, gold, and iron oxide can be exploited in novel imaging techniques to identify atherosclerotic plaques [23].

Vascular endothelial growth factor (VEGF) as well as the VEGF receptor (VEGFR) and integrin $\alpha_v\beta_3$, due to their important role in angiogenesis and tumor growth, can be applied in cancer diagnostic and therapeutic goals [24-26]. Indium-111 (^{111}In) labeled perfluorocarbon nanoparticles for single photon emission tomography (SPET) imaging of integrin $\alpha_v\beta_3$ in lung carcinoma angiogenesis have revealed that more ^{111}In atoms per nanoparticle reflects an increase in tumor-to-muscle ratio and mean tumor activity [27]. Therefore, this method may be an ideal method to identify newly developed tumors, especially when combined with other techniques [27]. The chemical and biological advantages of nanomaterials make them useful for the transport of contrast agents for nuclear imaging such as ^{99m}Tc , gadolinium, and fluorophores [7].

Quantum dots-based probes, combined with near-infrared fluorescence imaging (NIRF) and positron emission tomography (PET) of integrin $\alpha_v\beta_3$, have quantitatively improved tumor targeting efficacy, so that QD-based NIRF/PET imaging can detect tumors at a lower concentrations than those needed for *in vivo* NIRF imaging [14, 18, 28]. Quantum dots are suitable nanoparticles for cell tracking, reticuloendothelial system mapping, and tumor targeting [29]. Quantum dot-based dual functional NIRF and PET imaging has been applied to evaluate U87MG tumor targeting efficacy [29]. For this purpose, an amine-functionalized QD was linked to VEGF and macrocyclic 1,4,7,10-tetraazacyclododecane-N,N',N'',N''-tetraacetic acid (DOTA) for VEGFR specific binding after ^{64}Cu -labeling for PET imaging. The results showed

Table 3. Diagnostic applications with radiolabeled nanoparticles

Nanoparticle	Radionuclide	Kind of imaging	Application
Iron oxide	^{111}In	γ -camera	Breast cancer in mice [69]
Iron oxide	^{64}Cu	PET/MRI	Tumor angiogenesis in animals [16, 70]
Iron oxide	^{124}I	PET/MRI	Lymph node imaging in rats [71, 72]
Iron oxide	^{18}F	Trimodel MRI/PET-CT/optical imaging	In vivo PET-CT imaging in animals [73]
Perfluorocarbon (PFC)	^{111}In	γ -camera	Tumor angiogenesis in rabbits [27, 74]
Carbon nanotube	^{125}I , ^{111}In , ^{86}Y	PET	Distribution in mice [1, 75-79], Targeting of integrin av β 3-positive tumor in mice [78], multimodality imaging and molecular therapy [27, 80, 81]
Quantum dots	$\text{Cd}^{125\text{m}}\text{Te/ZnS}$	SPET/CT	Quantitative measurement [82, 83]
Quantum dots	^{64}Cu	PET/NIRF	Tumor angiogenesis PET/NIRF imaging [28, 29, 84-86], human prostate cancer cells growing in live mice [30], nanocrystal HDL into apolipoprotein E in mice (atherosclerosis) [23, 51, 87]
Quantum dots	^{18}F	PET/optical imaging	In vivo multimodal imaging [88], sentinel node mapping [89], in vivo fluorescence imaging (FLI) of the reticuloendothelial system [90]
Liposomes	$^{99\text{m}}\text{Tc}$, ^{111}In , ^{67}Ga ,	γ -camera	Detection of tumor, infection, inflammation, and lymphoscintigraphy [36, 91-94]
Liposomes	^{111}In	SPET	Clinical biodistribution and also imaging of breast, head and neck, glioma and lung cancers [95, 96], in C-26 tumor-bearing BALB/cByJ mice [36]
Liposomes	^{18}F	PET	In vivo tracking [97-99]
Liposomes	^{111}In , ^{177}Lu	SPET	Tumor targeting for C26 and HT29/luc animal model [98, 100, 101]
Liposomes	^{64}Cu	PET	Targeted delivery and imaging with bioconjugated ^{64}Cu -BATPEG-liposome [102]
Immunoliposome	^{111}In	γ -camera	Tumor visualization of murine lewis lung carcinoma and human HT-29 tumors [103-105]
Polymer	$^{99\text{m}}\text{Tc}$	γ -camera	Tumor angiogenesis [106]
Dendrimers	^{76}Br	PET	PET imaging of angiogenesis [107]

that the QD-based combination of NIRF and PET imaging significantly enhanced accuracy for the quantitative targeted NIRF imaging [19, 30-32].

Bifunctional PET/MRI imaging of integrin expression using polyaspartic acid (PASP)-coated iron oxide (IO) (PASP-

IO) nanoparticles linked to DOTA and cyclic arginine-glycine-aspartic (RGD) peptides resulted in accurate detection of tumor cells in initial stages [16]. The detailed application of radiolabeled nanoparticles in diagnosis is described in Table 3.

Research and preclinical applications of nanotechnology in therapeutics

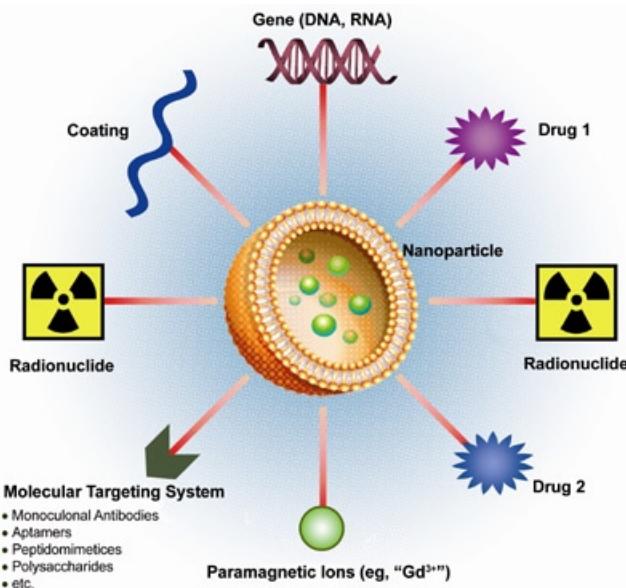
Currently peptides, viruses, and monoclonal antibodies against tumor molecules are being examined in research and applied as vehicles for specific tumor targeting and effective drug distribution [11, 33, 34]. In addition, several nanoscale liposomes, water-soluble polymers, micelles, and dendrimers are used as nanocarriers in nuclear medicine for diagnostic, therapeutic, and for both diagnostic and therapeutic (theranostic) goals [35][36]. Various genes [37], peptides [38], proteins [39] and antibodies can be tagged with carbon nanotube (CNT) vehicles to target tumor cells [40].

Carbon nanotubes are ideal for drug delivery because they have the ability to transfer effective quantities of radionuclide or drugs [41].

Others used ^{188}Re -(S₃CPh)₂(S₂CPH) [^{188}Re -SSS] [(bis(perthiobenzoato)(dithiobenzoato) rhenium-III)] trapped in lipid nanocapsules (LNC) as a novel radiopharmaceutical carrier for internal radiotherapy of malignant glioma in Fischer rats. They observed that LNC enhanced the tendency of ^{188}Re to remain in brain tissue. Furthermore, the median survival time of the rats treated with ^{188}Re -SSS LNC was 80% longer than the control group. They proposed that the lipophilic nature of LNC assists in more effective tumor irradiation [42].

Others functionalized epidermal growth factor (EGF) with diethylenepentaacetic acid (DTPA), tagged it with ^{111}In , and used it for the treatment of breast cancer. They observed that the growth rate and survival of hormone-resistant breast cancer cells was significantly reduced [41]. Others functionalized single-walled CNTs with amine groups and DOTA chelating groups.

Chimeric monoclonal antibodies against the CD20 epitope (rituximab) were then appended to the CNT-(DOTA) complex, and tagged with ^{111}In . This bifunctional nanostructure enabled selective targeting of Burkitt's lymphoma cells [43].



As for theranostics [32] the production of multifunctional nanoparticles has achieved a combination of diagnostic and therapeutic goals simultaneously [44]. Nanomaterial can target a specific site, transport information from the targeted cells, and deliver definite amounts of drug [45-47]. This multifunctional nanoplatforms of nanomedicine seems to play an important role in future [1] (Fig. 4).

Others administered cuprum-64 (^{64}Cu)-labeled folate-conjugated shell cross-linked nanoparticles for PET imaging and radiotherapy of tumor cells [48]. Others placed super-paramagnetic iron oxide nanoparticles (SPION) and ^{18}F -fluoride in haemagglutinating virus of Japan envelope (a vector for gene transferring) and compared their distribution with unaltered HVJ-Es when magnets were placed on the heads of injected rodents during PET scanning. It was revealed that magnetic force could change the biodistribution of the viral vehicle. Antibody (mAb)-linked iron oxide nanoparticles (bioprobes) heated by an applied alternating magnetic field (AMF) help to use in tumor specific thermal therapy (Rx) for metastatic cancer (Fig. 5) [49]. This control of biodistribution of therapeutic vehicles has made the site-specific delivery of genes, drugs, and tracers possible [50]. Others have reviewed different nanotechnology applications in molecular imaging and treatment of cardiovascular diseases [51]. Viral vehicles, due to their capability to combine with cell membranes, have been examined for gene delivery [52]. In this field, others studied the M13 virus aimed to help in cancer field [53]. M13 as well as other phages stick to multiple materials. Others have tried to bind M13 to cancer cells at one side and nanodevices known as quantum dots at the other side which could be applied in cancer diagnosis in medical body scans [54]. The detailed application of radiolabeled nanoparticles in treatment is described in Table 4.

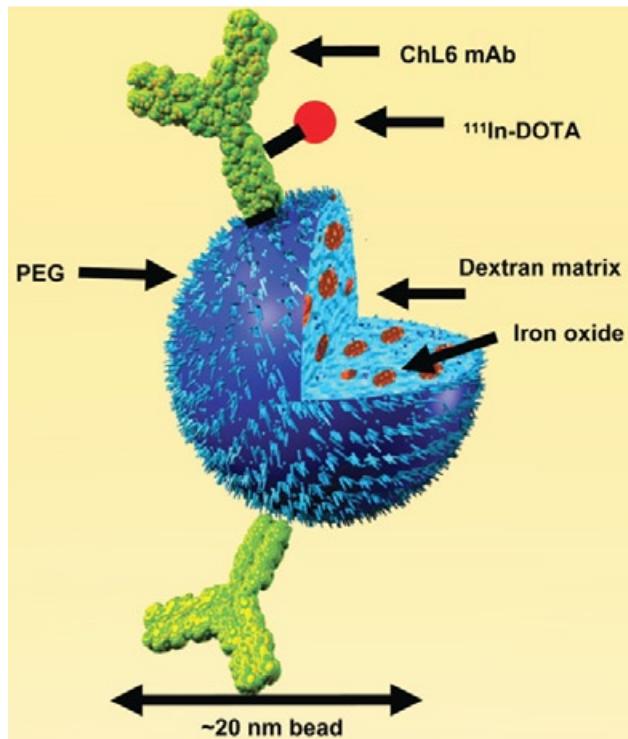


Figure 5. ^{111}In -labeled ChL6 antibody was conjugated to a dextran bead coated with polyethylene glycol and permeated with iron oxide nanoparticles. (Reprinted with permission from [49]. ©2007 Society of Nuclear Medicine)

Table 4. Therapeutic applications with radiolabeled nanoparticles

Nanoparticle	Radionuclide	Treatment	Application
Liposomes	^{131}I , ^{67}Cu , ^{198}Au	Radiotherapy	Internal radiotherapy [108-111], nude mice bearing human liver cancer [112], pre-targeted immunotherapy [113], breast cancer [94, 108, 110, 114, 115]
Liposomes	^{90}Y	»	Internal radiotherapy [89, 116-118]
Liposomes	^{186}Re	»	Radionuclide therapy in a head and neck squamous cell carcinoma xenograft positive surgical margin model [119-122]
Liposomes	^{188}Re	»	Ovarian cancer [114], colon cancer in mice [123, 124], internal radiotherapy [8, 124-130]
Liposomes	^{111}In , ^{186}Re	»	Therapeutic efficacy studies of ^{111}In / ^{188}Re -liposome on C26 and HT-29 tumor-bearing animal models [123, 131, 132]
Liposomes	^{225}Ac	»	Therapeutic agents for micrometastases cancer [133-136]
Liposomes	^{10}B	»	^{10}B -liposomes nanotargeted therapeutics for boron neutron capture therapy (BNCT) [137, 138]
Liposomes	^{111}In , ^{188}Re	Radiochemotherapy	Imaging, biodistribution, pharmacokinetics, therapeutic efficacy, and dosimetry studies of ^{111}In / ^{188}Re -VNB/DXR-liposome on C26 and HT-29 tumor/ascites-bearing animal models [122, 124, 129, 130, 132, 139, 140], rat brain tumor model [141]
Immunoliposomes	^{90}Y	Radiotherapy	Therapy with nanotargeted therapeutics of ^{90}Y -DTPA-liposome-IA(integrin antagonist) or ^{90}Y -DTPA-liposome-mAb [118]
Immunoliposomes	^{225}Ac	»	Micrometastases cancer [133-136]
Immunoliposomes and Folate-dendrimers	^{10}B	»	^{10}B -immunoliposomes-anti-EGFR and ^{10}B -PAMAM dendrimers-anti-folate nanotargeted therapeutics for boron neutron capture therapy (BNCT) [142, 143]
Streptavidin	^{111}In	»	^{111}In labeled 3-component streptavidin (^{111}In -MORF/tat/trastuzumab) nanoparticles for auger electron induced antisense-mediated cytotoxicity of tumor cells [144]
Dendrimer	^{198}Au	»	melanoma mouse model [145]

Applications in regenerative medicine

Regenerative medicine uses stem cells, induction of endogenous repair mechanisms, or transplantation to restore and repair inefficient tissue with functionality to treat debilitating disorders such as cancer, diabetes, cardiovascular, central or peripheral nerve damage, and osteoarthritic diseases [55, 56].

Quantum dots (QD), iron oxide (IO) nanoparticles, and nano-polymers are favorable materials for regenerative nanomedicine. They can be fused with radioisotopes and used for nuclear-medical procedures. Quantum dots are made from a heavy-metal core cadmium selenic (CdSe), telluric

cadmium (CdTe) encircled with a sulfuric zinc (ZnS) shell [56]. The thickness of the shell can be prepared depending on the reaction time.

Semiconductor nanocrystals like QD are used for cell labeling, cell tracking, imaging and monitoring of cellular events [57]. Furthermore QD can mark multiple parts of cells synchronously and can be used in multiplex imaging for biological application [58, 59]. They are also a good option for long-term labeling of stem cell progenitors [58].

Iron oxide nanoparticles can bind to external cell surfaces and easily separate, or can penetrate into a cell without affecting its viability [60]. A dextran-coated superparamag-

netic iron oxide (SPION) is an appropriate contrast agent for labeling human mesenchymal stem cells (MSC) and human embryonic stem cells (ESC) [61]. Others successfully determined the site of damaged brain cells after brain trauma in a human patient using mesenchymal stem cells (MSC) labeled with superparamagnetic iron oxide (SPION) [62]. Recent studies of SPION-labeled stem cells in cardiovascular system have been promising [63].

Artificial extracellular matrixes, which mimic the structure of natural matrixes, have a critical role in tissue engineering [64]. Nano-fibrous scaffolds function as a mechanical trellis, and can increase the survival of implanted stem cells, which are the key operators in regenerative medicine. They also help to determine the location of transferred stem cells or even can monitor their proliferation, differentiation, and viability [65, 66]. Sodium iodide symporter (NIS) is a membrane protein which can facilitate ^{99m}Tc -pertechnetate imaging [65]. For instance, a research group combined regenerative medicine with nanotechnology and nuclear medicine [65]. They designed MSC expressing the human NIS gene which has been used to estimate the viability of transplanted human stem cells. Scintigraphy has indicated that radionuclide uptake of an MSC-NIS/ poly L-lactic acid (PLLA) complex was higher than MSC-NIS not implanted in a scaffold. Mice treated with an MSC-NIS/PLLA scaffold mixture exhibited higher survival rates than controls treated with non-scaffold MSC-NIS. Scaffold of NSC-fluc/polymer and MSC-NIS/polymer scaffold complexes are valuable candidates for serial *in vivo* imaging and can be used for longitudinal monitoring of implanted stem cells [65].

The final aim of nanomedicine is that nanoparticle-based agents could be utilized for simultaneous diagnosis and treatment (theranostics), although much remains to be done before nanomedicine can be used in clinical practice [67, 68] (Fig. 6).

In conclusion, nanotechnology in our days is a broad field for medicine and nuclear medicine theranostics, which is expected to yield practical applications in the future.

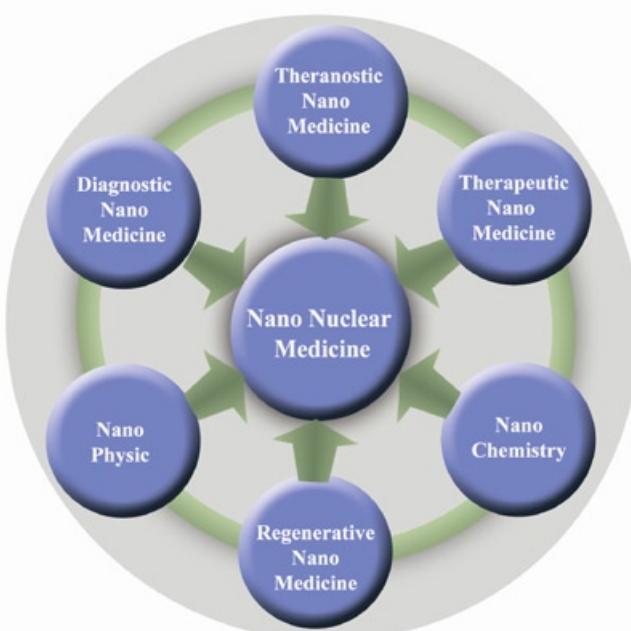


Figure 6. The proposed nano-nuclear medicine and related fields

The author(s) declare that they have no conflicts of interest.

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